Dosimetric materials applications – TSL and OSL

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Always measurement of dose. Not always boring! Always measurement of dose. Not always boring!

List of (selected) applications

- Personal dosimetry
 - Dosimetry in space
 - Neutron dosimetry
- Emergency dosimetry
- Enviromental monitoring
- Dosimetry in medicine
 - Radiotherapy
 - Radiodiagnostics
- Thermoluminescence dating
- Aplications in biology, reactor engineering, industry...
 - High dose measurement exploit OSL/TSL materials but use alternative means of evaluation
 - Optical absorption
 - Different TSL peaks
 - Radiophotoluminescence
- Military applications (Dr. Janda)
- Education
 - Lectures on thermolumiscence materials especially

Personal dosimetry

- Task
 - Measurement of a dose obtained by individual worker
- Requirements and their reasons
 - Small dosimeter
 - Wearable
 - Finger dosimeter (extremity dosimetry)
 - Eye dosimeter
 - Measurement range at least 0.1 mSv 1 Sv (10 Sv for extremities]
 - Natural background
 - Very roughly 1 mSv/year (radon not included) \rightarrow 0.25 mSv/evaluation period
 - Worker limit
 - 20 mSv/year (whole body, eye)
 - 500 mSv/year (skin, extremities)
 - Death
 - Approximately 4 Gy

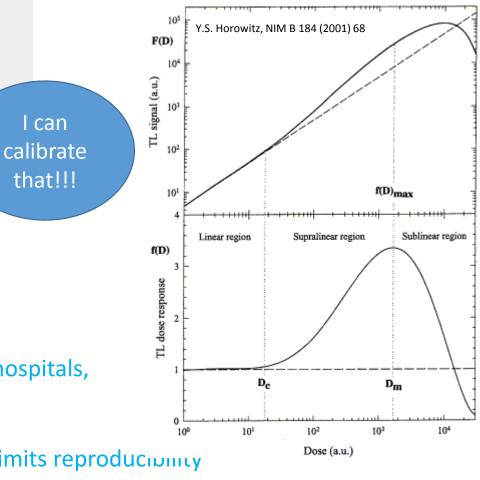




Personal dosimetry

- Requirements and their reasons
 - Low fading
 - Maximally 5 % during evaluation period (1 or 3 months)
 - Possibility of one-time irradiation (anytime)
 - Cheap, re-usable, fast reading, simple evaluation
 - High number of radiation workers (e.g. 12 000 in Czech hospitals, 1 000 000 in EU)
 - Linear dose response
 - Supralinearity and sublinearity complicates calibration, limits reproducionary
 - Response independent of (survivable) temperature, humidity, angle, energy, dose rate...
 - Acceptable precision
 - Approximately ±30(40) %
 - Low precision is mostly due to complex relation of $\rm H_{\rm p}(10)$ and dosimeter dose

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Just give me some time for all those necessary points

Personal dosimetry

• Limits are given in effective dose E

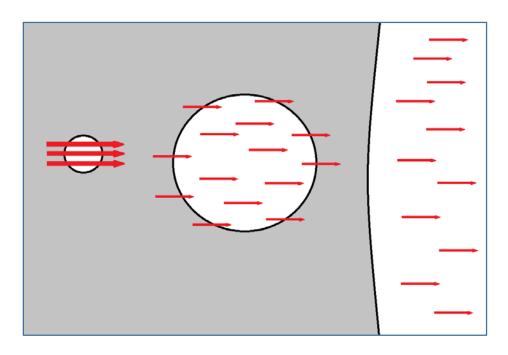
$$E = \sum_T W_T \cdot H_T = \sum_T W_T \sum_R W_R \cdot ar{D}_{T,R}$$

- $D_{T,R}$ dose in organ T from radiation R
- W_R radiation weighting factor
- W_T tissue weighting factor
- \rightarrow Should we measure $D_{T,R}$ for all organs and radiation type?
- Unrealistic!!!
- We measure Personal dose equivalent $H_p(10)$, $H_p(0.07)$ or $H_p(3)$
- Realistic assumption: $H_p(10) > E$

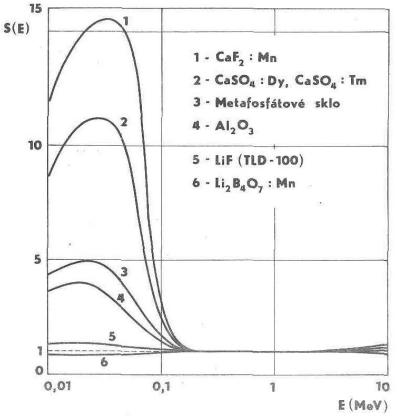


- For photon radiation and homogeneous irradiation
 - $E = H_p(10) = D$
- Approximation: R = c D
 - c calibration constant
 - D dose
 - R response
- So simple? Not at all...
- Dose
 - Absorbed energy / mass (Gy = J/kg)
- We measure D_{dos} dose in dosimeter
- We are interested in personal dose (in tissue) D_{T}
- We require $D_T = f D_{dos}$
 - Fortunately true
 - f (cavity correction factor) could be calculated or measured (calibration)

- Cavity theory (W wall = tissue; C cavity = dosimeter)
 - Assumption: photon beam / field is not attenuated
 - Otherwise detector irradiation is inhomogenous
 - Extreme: only shallow layer below surface is irradiated
 - High angular dependence
 - Small
 - $f = f_{small} = {}_{m}S_{C}/{}_{m}S_{W}$
 - Large
 - $f = f_{large} = (\mu_{En}/\rho)_C/(\mu_{En}/\rho)_W$
 - Intermediate (according to Burlin)
 - $f = d f_{small} + (1-d) f_{large}$
 - d = [1 exp(-Bx)] / Bx
 - B effective mass attenuation factor for electrons
 - x mean electron path in C
- Quantities dependent on photon energy
 - ${}_{m}S_{C',m}S_{W'}$ (μ_{E}/ρ)_C, (μ_{E}/ρ)_{W'}, B, x
 - \rightarrow f depends on energy

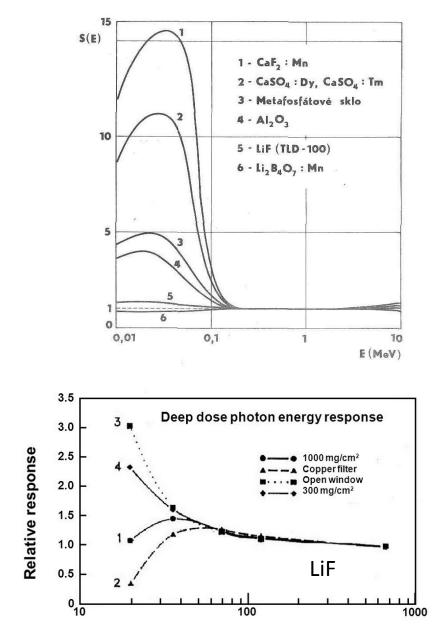


- Real TSL/OSL dosimeter could be considered small, intermediate or large cavity, depends on photon energy
- $D_T = f(E) D_{dos}$
- 😕 Energy E is generally unknown
- Solutions
 - Somehow make f constant
 - Compensate for the energetic spectrum
 - "Measure energy"



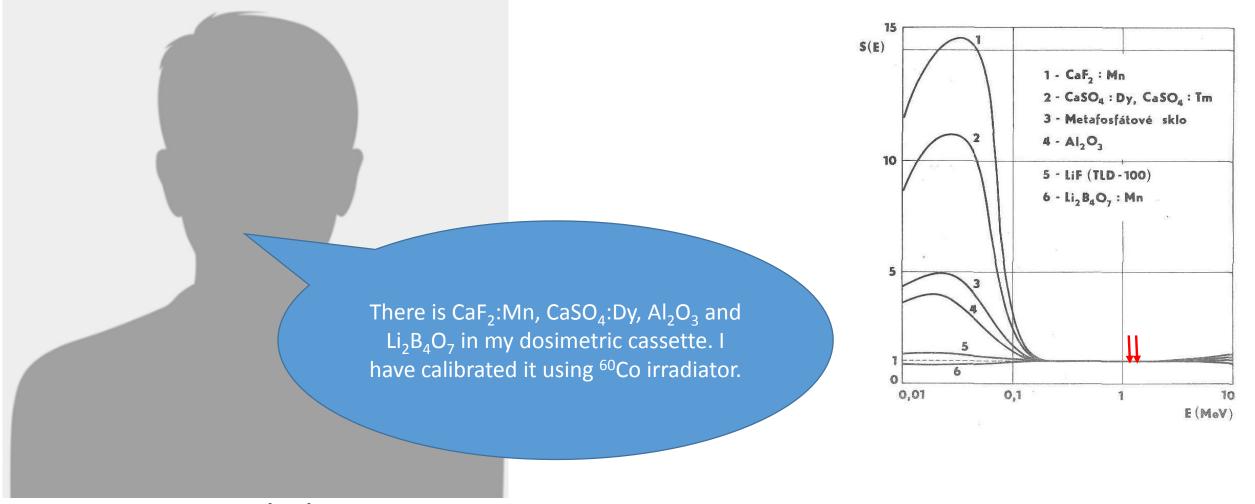
Personal dosimetry ("making f constant")

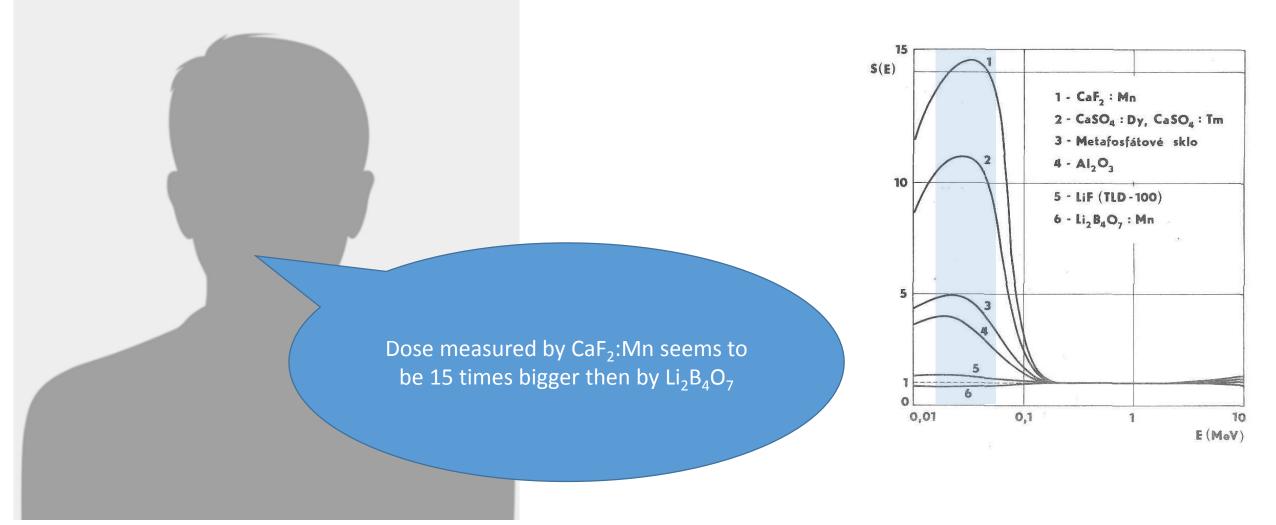
- f = d f_{small} + (1-d) f_{large}
 f = 1 if
 - $f_{small} = {}_{m}S_{C}/{}_{m}S_{W} = 1$
 - $f_{large} = (\mu_{En}/\rho)_{C}/(\mu_{En}/\rho)_{W} = 1$
 - d ≠ 1
 - Could be achieved for limited E interval
- So-called tissue equivalent materials
 - Close to tissue equivalence: LiF, Li₂B₄O₇
 - Far: far to many, e.g. CaF₂, CaSO₄
- Filtering methods

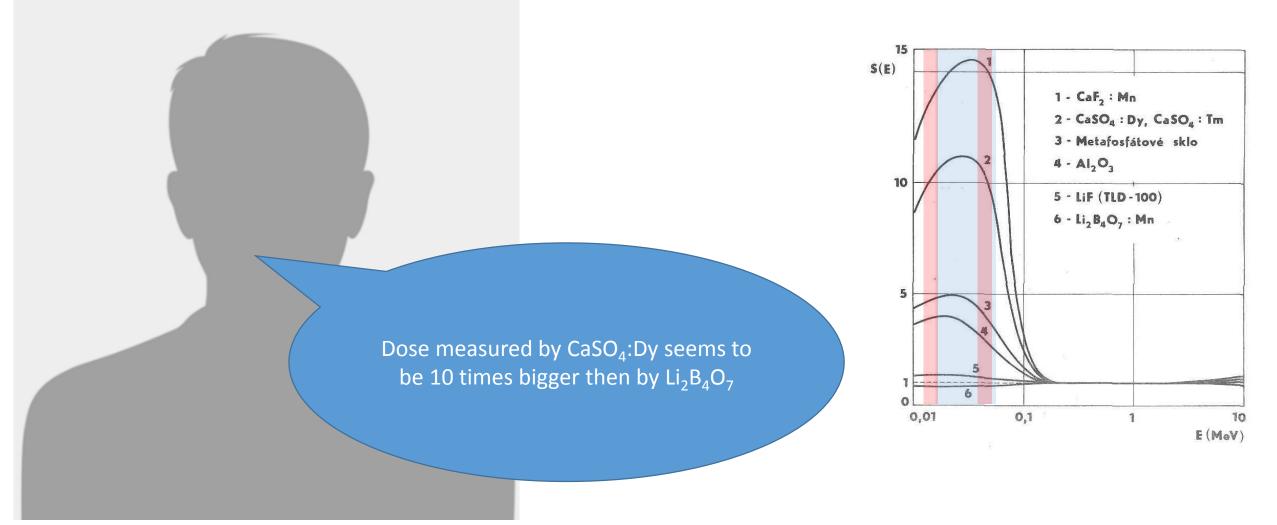


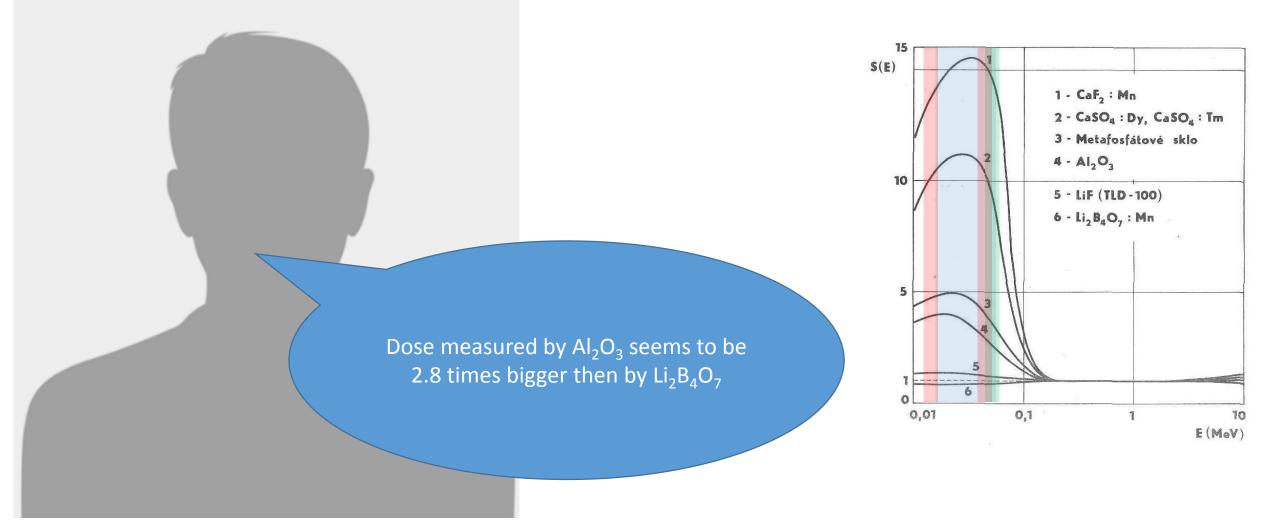
Photon energy - keV

J. Anderson, ASSESSMENT OF OCCUPATIONAL EXPOSURE DUE TO EXTERNAL RADIATION SOURCES AND INTAKES OF RADIONUCLIDES Personal Dosimeters, IAEA







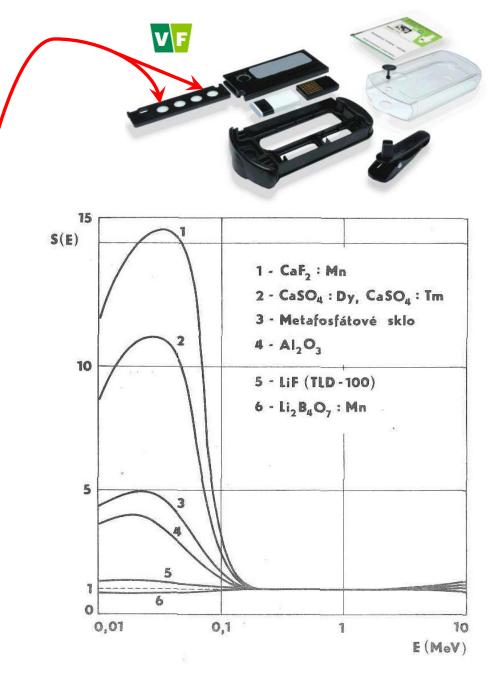




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This is a simplified example for a discrete energy spectrum. However, such analysis is in principle applicable for complex spectra as well (in a slightly more complicated form)

- Constant f
 - More simple
 - Faster evaluation (1 dosimeter)
 - Cheaper
- "energy measurement"
 - Rough information on energy available
 - Complicated evaluation if two or more materials are used
 - instead: one material, several dosimeters with different filters (probably most common method)
 - E.g., plastic, **plastic**, Al+plastic, Cu+plastic
 - Higher Z materials could be involved



Personal dosimetry (materials used)

• TSL

- LiF:Mg,Ti (MTS)
- LiF:Mg,Cu,P (MCP)
- CaF₂:Mn
- Li₂B₄O₇
 - Hygroscopic, closest to tissue equivalence
- Others...
- OSL
 - BeO
 - Linear 0.01- units Gy, dose underestimation for low photon energies (filtering is the solution), extremely low fading
 - Al₂O₃:C
 - 0.05-10 Sv, reproducibility (10 % signal loss after 25 cycles)

Personal dosimetry – advantages / disadvantages

- Advantages
 - Re-usable
 - Relatively cheap
 - Small
 - Simple measurement automatization
 - Large dynamic range
- Disadvantages
 - Hard to identify
 - One (or few) reading(s)
 - No possibility of contamination idetification
 - No possibility of ide
 - Fading (can be very small)
 - More filters → more detectors

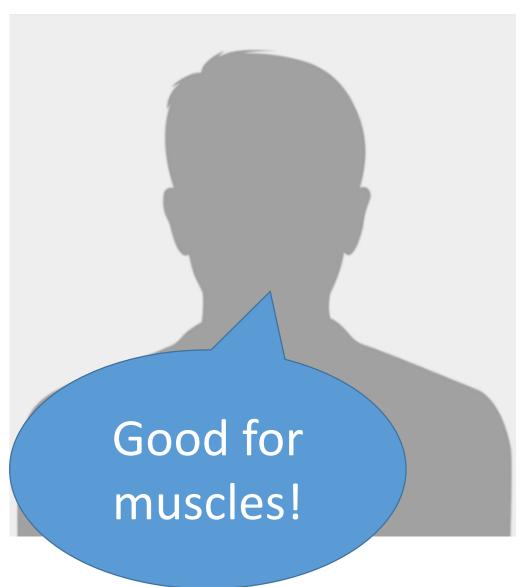
Personal neutron dosimetry – albedo dosimeter

- Some facts...
 - TSL materials sensitive to thermal neutrons are available: Li₂B₄O₇, LiF, CaSO₄:Dy,Li
 - ${}^{6}\text{Li} + n \rightarrow {}^{3}\text{H} + \alpha$
 - ${}^{10}B + n \rightarrow {}^{7}Li + \alpha$
 - ¹¹B and ⁷Li are insensitive
 - \rightarrow compensation principle could be applied
 - Compensation
 - 2 detectors ⁶Li enriched, ⁷Li enriched (⁶LiF / ⁷LiF)
 - Same response caused by γ and β radiation
 - Different response caused by thermal neutrons
 - R (⁶LiF) R(⁷LiF) = R(thermal neutrons)
 - Thermal neutrons are negligible contributors to effective dose

Detector of something unimportant. I love it.

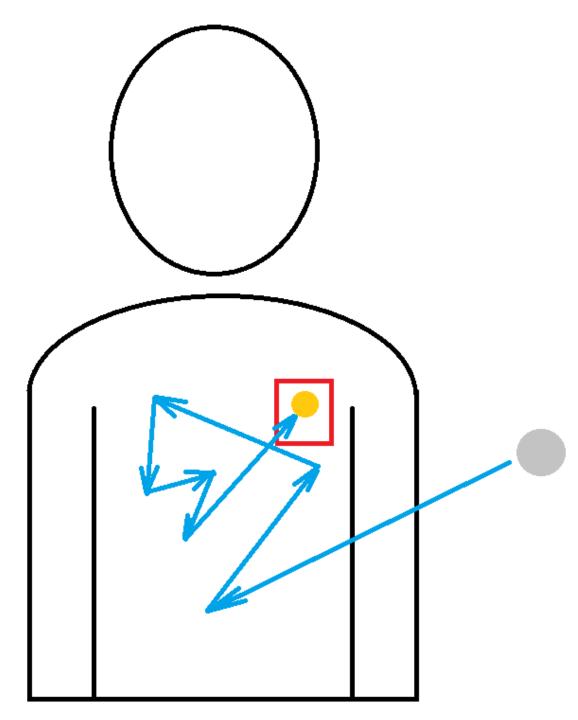
Personal neutron dosimetry – albedo dosimeter

- Some other facts...
 - Fast neutrons are important contributors to effective dose (if present)
 - Moderation
 - Fast neutrons \rightarrow thermal neutrons
- Eureka!
 - Solution: Moderator in TSL dosimeter vicinity
 - How much moderator?
 - Several kg should be enough



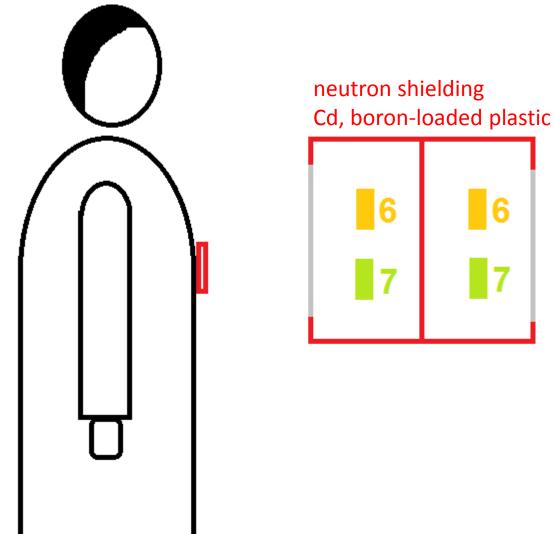
Actually...

Everyone carries several kg of moderator naturally...



Personal neutron dosimetry – albedo dosimeter

- R(thermal neutron) = R_{tn}
- Neutron $H_p(10) = C R_{tn}$
 - C calibration constant, (strongly) dependent on neutron spectrum
- Possibilities
 - 1) neutron spectrum is constant in time and known
 - One pair of dosimeters is enough
 - 2) spectrum of neutron source is known, but moderation is variable
 - Multi-element albedo dosimeter must be used
 - C is unambiguously dependent on ratio of responses albedo/direct
 - 3) different sources
 - Combination with other neutron dosimeters is necessary

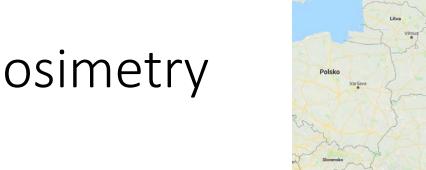


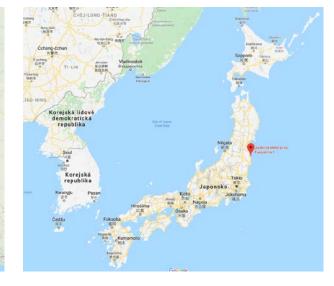
Enviromental monitoring

- Requirements similar to materials for personal dosimetry...
 - Dose range 0.1 mSv tens of mSv
 - Tissue equivalence welcomed
 - Able to withstand environmental conditions (higher/lower temperature, humidity)
 - Longer exposure period (up to 1 year)
 - Very low fading required
- Complex calibration, evaluation and correction procedure
 - Several sets of control dosimeters
 - Fading irradiation at site, but shielded
 - Response to zero dose not at site, not irradiated
 - Calibration irradiated by known dose, not at site

Emergency dosimetry

- Idea:
 - Accidents do happen
 - Higher dose \rightarrow higher risk \rightarrow higher need of medical examination
 - → we should know individual dose (2 Gy level considered a value dividing people as OK/needing intensive care)
 - General public members do not have dosimeters
- Application of naturally occurring TSL/OSL materials
- Application of artificial materials not produced as TSL/OSL materials, but having TSL/OSL properties
- People are surrounded by materials of various dosimetric properties
 - Investigate those properties
 - Choose the best materials
 - Optimize the methods of their evaluation





Emergency dosimetry - requirements

- Common materials
 - In every household
 - Optimal: anything carried all the time/most of the time by everyone
- Reproducible response
- Adequate dose range
- \rightarrow difficult problem
- Examples
 - OSL S. Sholom et al. Rad. Meas. 46 (2011) 1866
 - Linear response of all materials up to 3 Gy
 - Nails MMD₂₄ (minimum measurable dose) after 24 h 0.2-10 Gy
 - Only "dirty" nails produces signal (sand?)
 - Teeth MMD₂₄ 0.15-8.0 Gy
 - People love their teeth, in vivo measurement technique must be developed
 - Buttons MMD₂₄ 0.09-0.3 Gy
 - Some sensitive, some not
 - Credit cards MMD₂₄ 0.05-2.0 Gy
 - Some sensitive, some not

Emergency dosimetry

- Examples
 - S. Sholom, S.W.S. McKeever, RPD 170 (2016) 398
 - TL/OSL of mobile phones (integrated circuits in them)
 - Response linear up to 2 Gy
 - MMD 0.13-0.26 Gy
 - - If exposure time known, reconstruction possible
 - J.A. Ademola, C. Woda, E. Bortolin
 - TL response of tobacco dust
 - Probably contains some feldspar
 - Linear response 0.1-10 Gy

As a non-smoker, I find it unfair.

Radiotherapy (teletherapy)

- Energies used
 - kV beams (x-ray tubes)
 - ⁶⁰Co (1.17 + 1.33 MeV)
 - MV beams (linacs)
- Particles used
 - Almost exclusively photons
 - Protons application is on the rise
 - Neutron capture therapy seems to be not promising
- Applied doses:
 - Inside target volume tens of Gy
 - Outside target volume lower doses
- Other requirements
 - Tissue equivalence needed?
 - Arguments for yes: dosimetric casing should be small, always more precise, scattered radiation is present
 - Arguments for no: energies are known, very small energy dependence in used energy region
 - Linearity of response
 - Small size
 - Application in field of high dose rate gradient (IMRT); spatial resolution
 - No influence on radiation field (in vivo measurement); small thickness
 - Precision: ± 3 % (D; H_p(10))

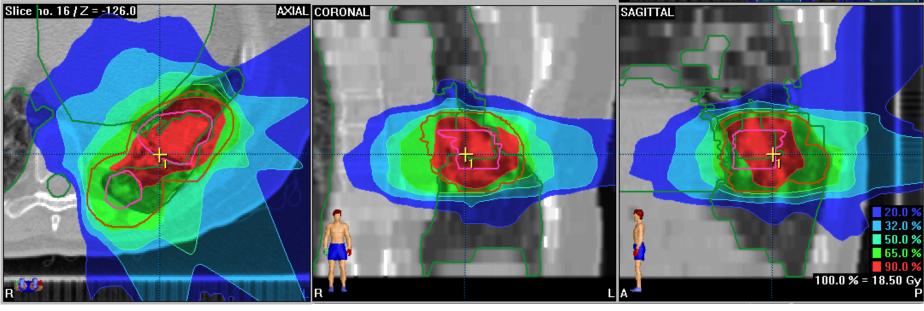
Radiotherapy

- Dose rates
 - Up tu Gy/min
- Contact with body
 - Temperature
 - Humidity
 - Body fluids
 - Sterilization
 - Non-toxic
- Measured quantities
 - Entrance absorbed dose
 - Machine output
 - Patient position
 - Exit absorbed dose
 - Delivered dose
 - Intracavitary absorbed dose
- Purpose

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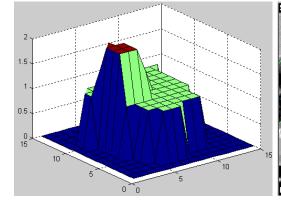
- Irradiation plan verification
- Type of measurement
 - Phatom measurement
 - Simple
 - Antropomorfic
 - In vivo measurement

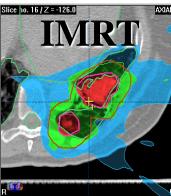
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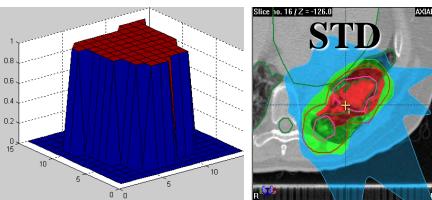


WP34 Calibration Water Phantom





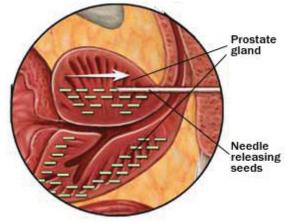




Radiotherapy – other modalities

- Brachytherapy
 - Used energies are small
 - Beta radiation is used
 - S. Kirov et al. Phys. Med. Biol. 40 (1995) 2015
 - ¹⁹²Ir dose distribution in water phantom; TLD-100 (LiF:Mg,Ti)
 - L.A. DeWerd et al. Rad. Meas. 71 (2014) 276
 - Determined precise energy dependence (1.04-1.13; $1.0 \approx {}^{60}$ Co)
 - ¹²⁵I, ¹⁰³Pd, ¹⁹²Ir used; measurement using TLD-100
- Nuclear medicine
 - Much more complicated
 - Short penetrating range of particles
 - Changing distribution of radionuclide in body through time
 - TL/OSL application has limited value





Radiodiagnostics

- Purpose
 - Determination of absorbed dose
 - \rightarrow intercomparison of departments using same modalities
 - \rightarrow Diagnostic reference levels determination
 - Justification, optimization (radiation protection)
- Energies
 - Up to 120 kV (skiagraphy, CT)
 - Around 200 keV (SPECT, Gamma camera)
 - 511 keV (PET)
- Doses
 - Abdominal CT, PET, SPECT approximately 10 mSv (Dual energy CT even higher)
 - Skiagraphy of joints, extremities 10μ Sv
- Measurements
 - In vivo
 - Antropomorphic phantoms
- Tissue equivalence important
 - Radiation field unchanged (energy in kV range)



CONCEPT-MIKE ADAMS ART-DAN BERGER WWW.NATURALNEWS.COM

CAUSE CANCER

DETECT

MAMMOGRAM 5000 CONTROL PANEL

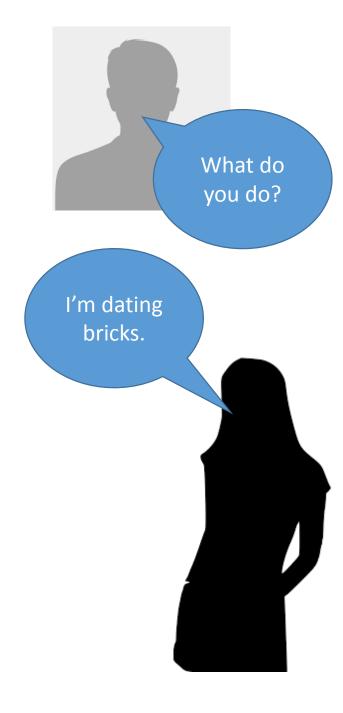


Thermoluminescence dating

- t = $\frac{D}{\dot{D}}$
 - t object age
 - D measured dose
 - *D* dose rate

• t = 0

- Moment of annealing, i.e. trap emptying
- = heating of the object
 - Firing of pottery, bricks, etc.
 - Fire burial
 - Fire



Thermoluminescence dating

- D is tricky
 - Supralinearity?
 - Sublinearity?
 - Fading?
 - Plateau test
- \dot{D} is tricky
 - Was it constant through the ages?
 - How can we measure it?

•
$$\alpha$$

• β
• γ
• γ
• γ

• cosmic

Thermoluminescence dating

 $\overline{k\dot{D}_{\alpha} + \dot{D}_{\beta} + \dot{D}_{\nu} + \dot{D}_{cosmic}}$

 D_{β}

neg

cosmic

 $\overline{k\dot{D}_{\alpha}+\dot{D}_{\beta}}$

- Techniques to make it easier
 - Quartz inclusion
 - Quartz α activity is low
 - Take large inclusion
 - Remove layer irradiated by α from outside
 - Fine-grain
 - Use only small grains (< 10 μm)
 - Everything is irradiated homogeneously
 - Subtraction dating
 - Fine-grain quartz
 - For objects removed from original environment (museum)
 - Zircon inclusion
 - High α activity

Thermoluminescence dating - faking

- TL dating is prone to be deceived by fakes
- Example from:

https://www3.nd.edu/~nsl/Lectures/phys10262 2014/art-chap5-4.pdf

- What dose is equivalent to 1200 yrs (clay horse T'ang dynasty)?
- 6.11 Gy
- What to do?
 - Combine methods they should not contradict themselves
 - Problem: one method = one sample; many methods = many samples \rightarrow object gone
 - Combine with non-invasive methods (e.g. archeomagnetism)